



# Laser spectroscopy of finite size and covering effects in magnetite nanoparticles

V N Nikiforov<sup>1</sup>, A N Ignatenko<sup>2</sup>, A V Ivanov<sup>3</sup> and V Yu Irkhin<sup>2</sup>

<sup>1</sup> M V Lomonosov Moscow State University, Moscow, Russia

<sup>2</sup> Institute of Metal Physics, Ural Division of RAS, Ekaterinburg, Russia

<sup>3</sup> N N Blokhin Russian Cancer Research Center, Moscow, Russia

E-mail: [ivavi@yandex.ru](mailto:ivavi@yandex.ru)

Received 22 July 2015, revised 12 November 2015

Accepted for publication 13 November 2015

Published 17 December 2015



## Abstract

Experiments on the impact of the size of magnetite clusters on various magnetic properties (magnetic moment, Curie temperature, blocking temperature etc) have been carried out. The methods of magnetic separation and centrifugation of water suspensions of biocompatible iron oxide nanoparticles (NPs) allow one to produce fractions with diameters of nanoparticles in the range of 4–22 nm. The size of the NPs is controlled by the methods of dynamic light scattering (DLS), transmission electron microscopy (TEM) and atomic force microscopy (AFM). For the first time the DLS method is applied in real time to control the size during the process of the separation of the NPs in aqueous suspensions. The changes of the size of NPs cause a shift in the Curie temperature and changes in the specific magnetic properties of the iron NPs. The experimental data is interpreted on the basis of Monte Carlo simulations for the classical Heisenberg model with different bulk and surface magnetic moments. It is demonstrated experimentally and by theoretical modeling that the magnetic properties of magnetite NPs are determined not only by their sizes, but also by their surface spin states, while both growing and falling dependences of the magnetic moment (per  $\text{Fe}_3\text{O}_4$  formula unit) are possible, depending on the number of magnetic atoms in the nanoparticle. NPs that are both clean and covered with bioresorbable layer clusters have been investigated.

Keywords: dynamic light scattering spectroscopy, magnetic nanoparticles, magnetite, magnetization, Monte Carlo simulations

(Some figures may appear in colour only in the online journal)

## 1. Introduction

A method of laser correlation spectroscopy, namely dynamic laser scattering (DLS), is used in nanotechnology for reliable control of the size of nanoparticles (NPs) in real time, including the actual chemical and biological processes [1–3]. Nanoscale magnetic materials are of particular interest for applications in ferrofluids, high-density magnetic storage, high-frequency electronics, high-performance permanent magnets and magnetic refrigerants. The magnetism of NPs is an area of intensive development which impacts various areas of research including materials science, condensed matter physics, biology, medicine, biotechnology, planetary science, and so on [4–6]. In particular, iron oxide colloids have a low

toxicity and manifest good biocompatibility, which makes them applicable in various areas of medicine, e.g. for drug delivery systems and for hyperthermia treatment of cancer. For use in magnetic separation, MR tomography, magnetic hyperthermia and other applications [7], the methods of metrological control of magnetic NPs have been developed [8]. Today this is quite a difficult task, since in the 1–10 nm size range many of the techniques used are at the limit of their resolution, and the data obtained by different methods do not always correlate. For drug development, the most difficult question is the control of the size of the particles and, in the first place, the size of these objects in native fluids. The key techniques for the creation of the composite materials to be used in oncology are based on the fact that the typical range for their size

allows them to accumulate selectively in malignant tumors as compared to healthy tissue, in which the affected area is irradiated in a certain spectral region [7]. So, the dispersion of nanoshells should be strictly limited to a narrow region.

The increasing interest in nanoobjects is associated with the manifestation of the so-called ‘quantum size effects’. These effects take place with the decrease of the size of the particle and with the transition from a sample of macroscopic size to a sample size of a few hundreds or thousands of atoms, when the electron spectrum in the valence and conduction bands changes sharply. This phenomenon affects the electron and magnetic properties of the particles. The continuous spectrum presented at the macro-scale is replaced by a set of discrete levels, the distances between which are dependent on the size of the particles. Due to the size-dependency of the NPs, they are used for a new type of applications.

At present, it has been thoroughly confirmed by various studies that nanostructures (including nanoclusters) demonstrate a significant difference in many physical and physico-chemical properties in comparison with bulk materials [9, 10]. For example, nanocluster melting temperatures could be both above and below those of their bulk analogues [11–13].

As regards work in the field of physics of magnetic nanoclusters (see e.g. [14]), a number of models have been constructed and many experiments have been performed. However, systematic analysis of the conducted experiments has not yet been performed. Now, it is possible to believe to a large extent that the study of NPs leads to the necessity to accept two new arguments [9, 10]:

1. The elementary excitation spectrum of NPs is discrete owing to their small size.
2. The total number of surface states of a NP is comparable to the number of bulk ones.

The use of these two principles concerning ‘nanomagnetism’ can be realized by means of the ‘core-shell’ picture, which allows separation of the contributions of the surface and bulk states to the magnetic properties of a NP. In this letter these ideas are applied to iron oxide (magnetite) NPs. The models proposed earlier [8] include a phenomenological Weizsäcker model (by analogy with the Weizsäcker approach in nuclear physics) and microscopic Ising and Heisenberg models with modified surface magnetic moments. Our approach is based both on making experiments and constructing models. The experimental research deals with magnetite NPs synthesized by different methods. The DLS technique, supposedly, should have simple and effective scheme feedback, automatically adapting the power of the laser source and under study of a particular sample; improved characteristics of the receiving path for the input signal with a low noise amplifier and squelch; an efficient algorithm for decomposing the spectrum of the scattered signal power fluctuations into the components that characterize the individual (‘mono-disperse’) fraction of NPs presented in the system; this algorithm should include the possibility of simultaneous resolution of the integral equations describing the scattered signal for different scattering angles and regularization methods. Dynamic light scattering allows one to control the distribution of the size of inorganic

iron oxide NPs in suspension. Apparatus based on the DLS method allows one to control the production of nanomaterial at all stages of the technological cycle.

## 2. Materials and experimental methods

Native  $\text{Fe}_3\text{O}_4$  was synthesized according to the following method: firstly, particle sedimentation from iron salt solution mixed with sodium hydroxide at pH 10 – 12; secondly, activation in dilute HCl; thirdly, stabilization by treatment with dextran; and, finally, purification [15, 16].

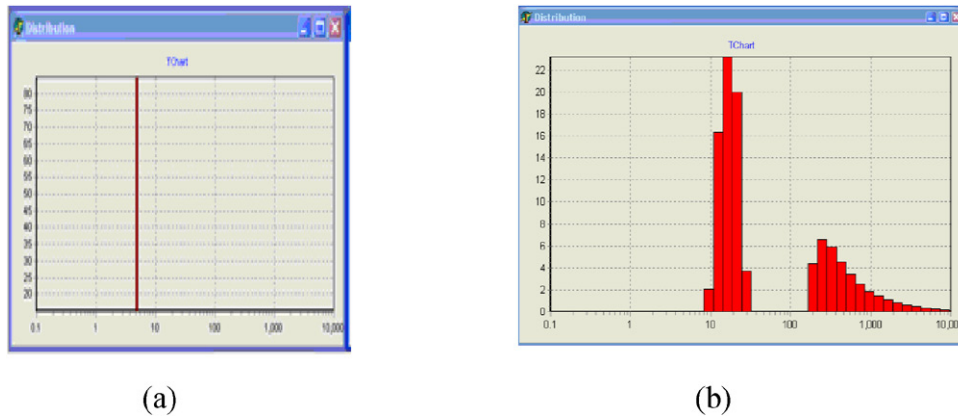
The iron oxide NPs were synthesized by co-precipitation [17]. To extend the region of superparamagnetic iron oxide NPs (SPION) sample sizes, the conditions of the synthesis were changed with careful control by transmission electron microscopy (TEM) and x-ray diffraction, while low-quality samples were eliminated [7]. SPION samples were coated by DNA [18] and by PVA [19, 20]. The NPs were stabilized *in situ* by organic surfactant molecules which acted both as a stabilizer of the microemulsion system and as a capping layer of the NP surface. The control of the NP size was attained by careful adjustment of the preparation conditions. The structure, morphology and distribution of the NP size were investigated by DLS, x-ray diffraction, TEM, atomic force microscopy (AFM) and scanning electron microscopy.

Physical and chemical characterization of initial precipitates,  $\text{Fe}_3\text{O}_4$ , dextran-ferrite and their suspensions were performed by the DLS laser technique KURS3M (figure 1), TEM, electron spin-resonance spectroscopy (ESR), magnetic measurements (by vibrating and SQUID magnetometers) and x-ray diffraction.

The diameter of magnetic NPs is the main parameter, determining their properties such as toxicity, biocompatibility, physical and chemical properties [7]. Nevertheless, the covering of NPs can also affect their magnetic properties. The DLS technique helps to detect, in real time, the changes in the size of NPs that, consequently, leads to a shift of the Curie temperature and specific magnetic properties of iron NPs. Magnetic separation [7] and centrifugation of the water suspension of biocompatible iron oxide NPs allows the production of ‘monodisperse’ fractions of NPs (figure 1, left) with different diameters (4 – 22 nm) controlled by the methods of dynamic light scattering, x-ray diffraction, TEM, atomic force microscopy (AFM) and scanning electron microscopy.

The TEM was performed using an EM-400 instrument (500.000x, a resolution of 0.4 nm) and a SEM IPS image analyzer. The crystal structure was depicted, and composition was controlled to avoid multiphase samples. Test results confirm the presence of one phase of the spinel structure, as well as the size of an average particle of 4 – 22 nm (by the Scherrer equation).

A particular effort was made to study the effect of the size and capping of the NPs on their magnetic structure. Magnetic diagnostics methods SQUID and ESR [21] were used. The temperature and magnetic field dependences on the magnetic moment were measured, and ESR spectra for NPs were obtained at temperatures of 4.2 – 380 K. Specific



**Figure 1.** Magnetic separation, centrifugation of a water suspension of biocompatible iron oxide NPs produces fractions with different diameters of NPs 4–22 nm controlled by the dynamic light scattering technique. The ‘monodisperse’ fraction (a) is shown on the left, on the right the source DLS spectrum (b) before treatment is presented.

saturation magnetization  $J_s$  of powder samples and their temperature dependence at 10–700 K was determined on a vibrating-sample magnetometer with a sensitivity of  $10^{-5}$  A m<sup>2</sup> kg<sup>-1</sup> in an applied magnetic field of about 0.75 T. ESR spectra in the 78–400 K temperature interval were collected. Temperature and magnetic field dependences were also measured at 4.2 – 350 K by SQUID and a vibrating sample magnetometer VSM PARC-155 as well as by Curie balance magnetometer.

### 3. Results of experiments

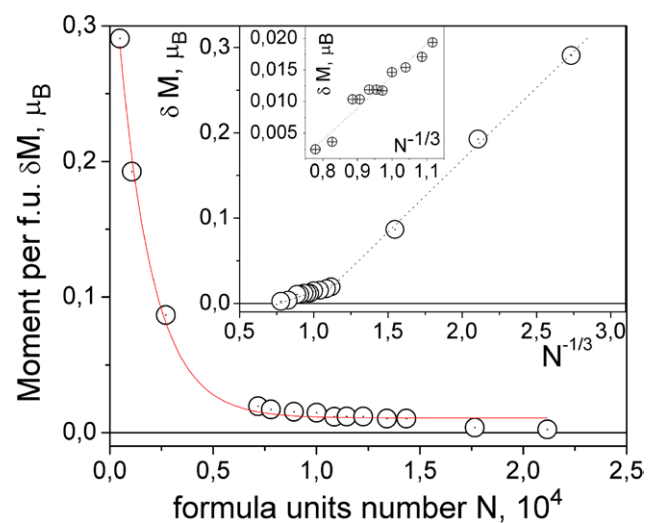
The distribution of magnetic NPs in size and their determined average size were obtained experimentally. The co-precipitation method enabled one to obtain the spectrum from 5 – 22 nm. The application of centrifugation, magnetic separation and shaking with ultrasound processing yielded fractions with specific dimensions.

In addition, coated iron oxide NPs in the polymer matrix have been investigated. According to TEM, AFM and DLS their size was 60 – 180 nm. Electron microscopy (SEM) demonstrated larger sizes (up to 225 nm). It should be noted that the true diameter of the magnetic NPs can be smaller by several times due to the passivating coating effect.

The average values of the effective magnetic moment per formula unit, the effective magnetic moment of one particle,  $\mu(N)$ , and the average number of formula units in one particle were estimated, as in [17, 21] from the Langevin expression  $M(H) \propto \mu(N) [\text{cth}(\mu(N)H/k_B T) - k_B T/(\mu(N)H)]$ .

The experimental results can be summarized as follows:

1. The specific magnetic moment of nanoclusters changes monotonically with the increase of particle size  $\mu(N)$  (see figure 1).
2. This monotonic dependence of  $\mu(N)$  can be either increasing (see figure 1) or falling (see figure 2) for different samples.
3. In dependences  $M(H)$ , the absence of hysteresis was observed, which indicates the absence of the coercive force and, consequently, the superparamagnetic state of NPs (see figure 3).



**Figure 2.** Deviation of magnetic moment per formula unit from the bulk value for magnetite 4 – 22 nm NPs (in Bohr magnetons) from the Langevin formula,  $T = 300$  K, measurement field 0.5 T. The inset demonstrates size dependence (diameter of NPs is proportional to  $N^{1/3}$ ) of the magnetic moment per formula unit for ultra-small (see right part of inset) and more large NPs (see left part of inset, and also the inset within inset).

4. Curie temperature gradually falls with the decrease of the NP size.

The dependence of the average magnetic moment change per formula unit in NPs was obtained. In our case, it was falling (see figure 2). However, in some cases one can observe dependence of the opposite type. With the increase in the diameter of iron oxide NPs subjected to surface treatment and sealed in a polymer matrix, the rise of the magnetic moment is observed with the increasing diameter of the NPs (see figure 4).

In the results presented here, the samples had the form of nanopowder. Moreover, a number of investigations of NPs in liquid were carried out.

A typical  $M-H$  (magnetization versus applied magnetic field) behavior of magnetic NPs in water is presented in figure 5. The calculated value of the magnetic moment of each cluster (according to the Langevin equation) is 6885

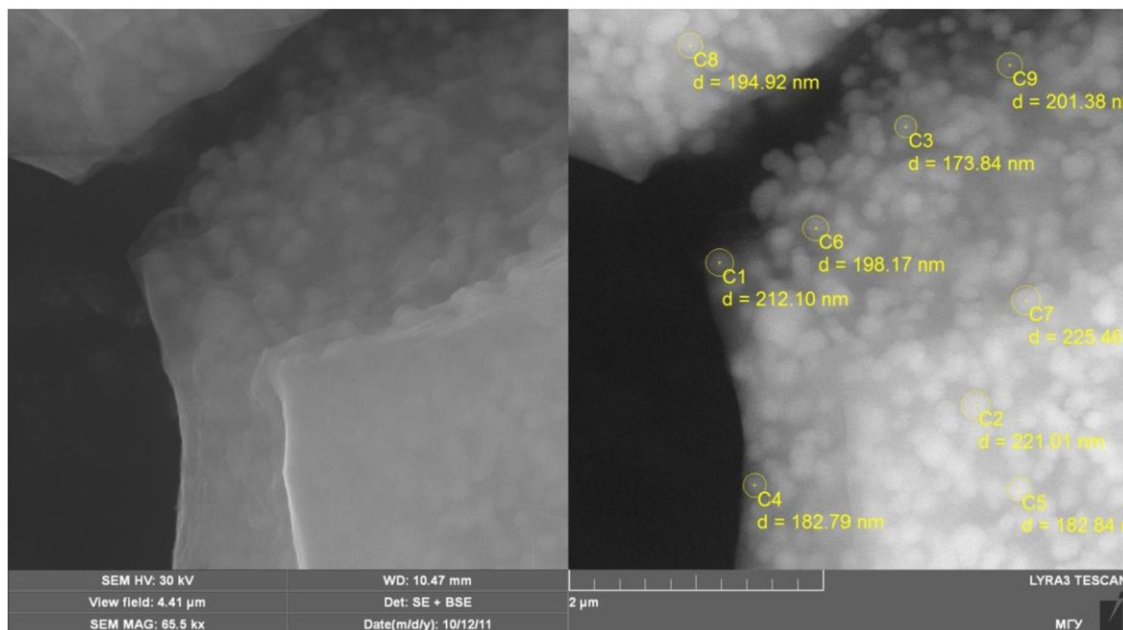


Figure 3. SEM image of the iron oxide NPs in a polymer matrix.

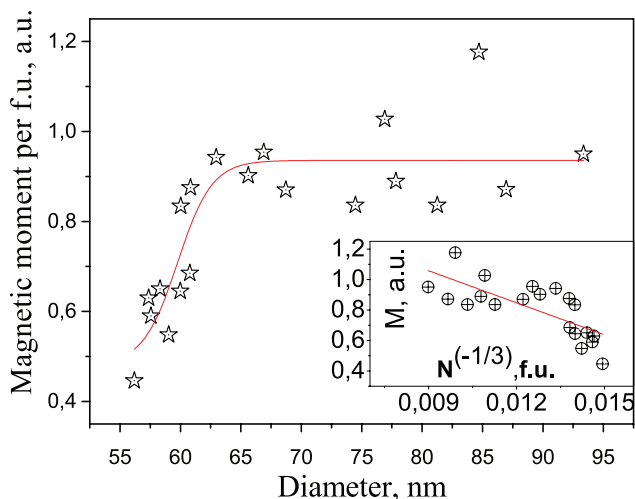


Figure 4. Magnetic moment per formula unit (in arbitrary units) versus diameter of magnetite NP in coated non-native iron oxide clusters in a polymer matrix (see below in figure 4),  $T = 300$  K. The inset shows magnetic moment versus  $N^{-1/3}$  dependence.  $N$  is the number of formula units per NP.

Bohr magnetons. The dependence with zero coercive force is a characteristic of superparamagnetic NPs.

The magnetic characteristics of NPs on the magnetite basis in the form of magnetic liquid, polymer matrix and quartz matrix were also investigated.

The temperature dependence of the zero field cooling (ZFC) and field cooling (FC) magnetization in a weak field of 2.27 mT is shown in figure 6. Note that the corresponding values of zero-temperature magnetization  $M_0$  are small. They increase rapidly with increase of the field (see e.g. figure 2 in [20]). In the case of bulk samples of magnetite, the Curie temperature is 580 °C, as confirmed by our experiments (figure 6 bulk curve). The temperature dependence of the magnetization of bulk samples from natural Urals magnetite and magnetite NPs with various sizes are shown in figure 6.

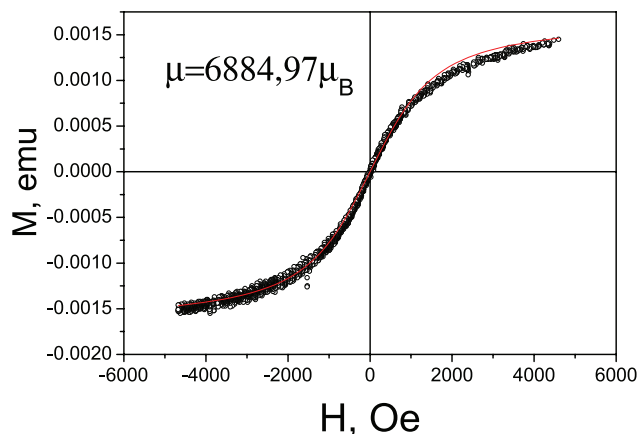
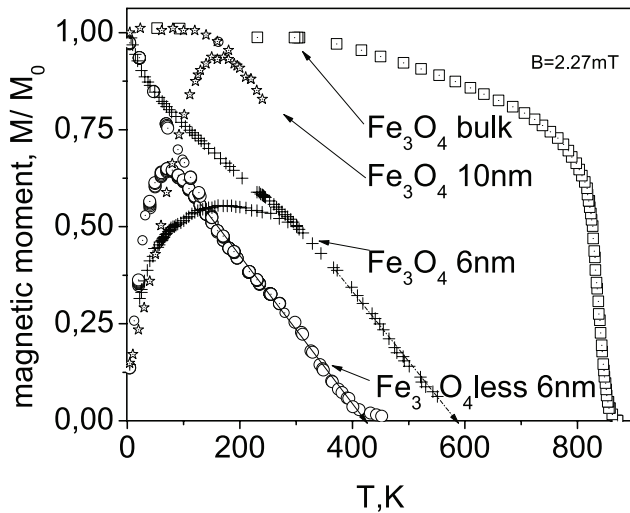


Figure 5. Magnetization versus applied magnetic field for dextran-coated iron-oxide NPs in water. The solid line shows the Langevin behavior.

The influence of the NP environment and conditions of the synthesis on the blocking temperature  $T_B$  (which corresponds to the maximum of the ZFC curve) were investigated. The dependence of  $T_B$  on the synthesis conditions was revealed. The SQUID magnetic diagnostic methods were used. The magnetic properties of NPs obtained by identical methods were studied by measuring the temperature dependence of magnetization  $M(T)$  and hysteresis in the  $M(H)$  curves. The temperature dependence of the magnetization  $M(T)$  in the ZFC mode (cooling in zero field and measuring with subsequent heating) and FC mode (the same in non-zero applied field) differ significantly (see figure 6).

Since  $T_B$  depends on the size of the magnetic NPs, it is promising to use this parameter for the metrology of magnetic NPs.  $T_B$  is usually related to the particle size while the constant of magneto-crystalline anisotropy  $K$  is defined by the equation  $K = 25 k_B T_B / V$ , where  $k_B$  is the Boltzmann constant and  $V$  the average volume of one NP. However, according



**Figure 6.** The temperature dependence of the relative ZFC/FC magnetization for bulk samples of magnetite ( $M_0 = 2.1 \text{ A m}^2 \text{ kg}^{-1}$ , squares) and for dextran-coated NPs with the sizes 10 nm ( $M_0 = 0.86 \text{ A m}^2 \text{ kg}^{-1}$ , asterisks), 6 nm ( $M_0 = 0.83 \text{ A m}^2 \text{ kg}^{-1}$ , crosses) and smaller than 6 nm ( $M_0 = 0.76 \text{ A m}^2 \text{ kg}^{-1}$ , circles).

**Table 1.** Effect of surfactants on the blocking temperature  $T_B$  in iron oxide NPs, where  $C_v$  is NP concentration.

$\text{Fe}_3\text{O}_4$	$T_B$
$\text{Fe}_3\text{O}_4$ PVS, $C_v = 1\%$	70.3 K
$\text{Fe}_3\text{O}_4$ PVS, $C_v = 1\%$ , $H = 0$	90 K
$\text{Fe}_3\text{O}_4$ liquid coll DNA	61.5 K
$\text{Fe}_3\text{O}_4$ polymer matrix	177 K
$\text{Fe}_3\text{O}_4$ glass	145 K

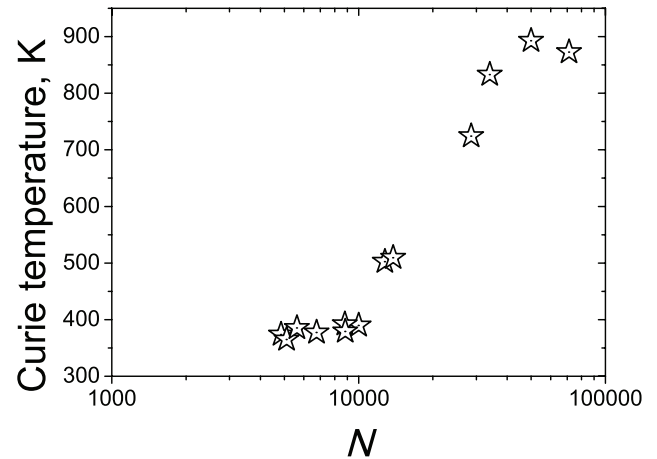
to our experiments, the size of magnetic NPs is not the only parameter determining the value of the blocking temperature (see table 1).

The passivation and drying of the NPs in zero magnetic field ( $H = 0$ ) increases the value of the blocking temperature  $T_B$  significantly (up to 20 K). The coating of magnetic NPs by biopolymers, in particular by DNA, is the factor that changes the surface contribution to the magnetic moment and, according to our experimental data, has a significant impact on  $T_B$  (see table 1). Coating of magnetic NPs by PVS and glass at various modes of passivation also affects the  $T_B$  value.

In the case of magnetic magnetite NPs the situation changes, namely, the Curie temperature decreases with the decreasing size of the NPs (see figure 7). The monotonic and size dependent Curie temperature is observed in native (non-coated) iron oxide NPs. The change of the synthesis conditions and size separation allow one to make variations in the diameter of magnetic NPs.

#### 4. Theory: core-shell model and Monte Carlo calculations

The experimental data presented can be interpreted on the basis of several different methods: various approximations in the Ising or Heisenberg models, quantum-chemical and first-principle calculations [22]. Of all these approaches, the



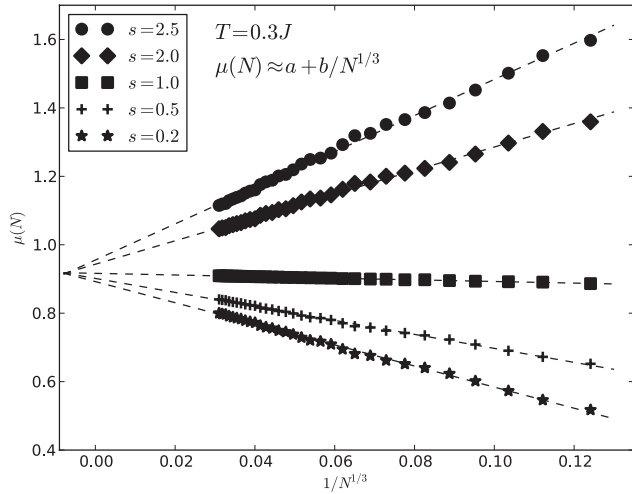
**Figure 7.** The size-dependent Curie temperature (in Kelvins) for the synthesized magnetite NPs.  $N$  is the number of formula units in each magnetic iron oxide NP.

core-shell model is regarded as the most suitable approximation [5]. It is a modification of the Weizsäcker model used for the analysis of specific characteristics of a complex nucleus. This model covers different bulk and surface magnetic moments (per atom) for a NP [8]. Some *ab initio* band calculations predict the enhancement of the magnetic moments in thin films as compared to the bulk value [23], and it is believed that the same outcome for the surface layers of NPs could be anticipated. However, the reduction of the saturation of magnetization  $M_S$  is a common experimental observation in many fine-particle systems [24]. In early models, this fact was interpreted by postulating the existence of a passive (i.e. ‘dead’) magnetic layer originating from the demagnetization of the surface spins, which causes a reduction of  $M_S$  [25]. A random canting of the surface spins caused by competing antiferromagnetic interactions between sublattices was proposed by Coey [26] for the purpose of the reduction of  $M_S$  in the maghemite ferrimagnetic particles.

The Weizsäcker model yields the equation for the magnetic moment  $\mu(N) = a + b/N^{1/3}$  [8]. To test this hypothesis we apply the Monte Carlo method. This approach enables one to obtain rather accurate quantitative results and is widely used in nanophysics now. In particular, a number of calculations for magnetically uniform clusters have been carried out [27–31].

The investigation of the surface effects in the magnetic NPs FePt was presented by Labaye *et al* [32]; the authors considered the effect of the surface anisotropy on an isolated single-domain spherical NP using atomic Monte Carlo simulation of the low-temperature spin ordering. The analogous behavior was found in the work [33] where the effect of surface anisotropy upon the magnetic structure of ferrimagnetic maghemite NPs was studied by applying the 3D classical Heisenberg–Hamiltonian and the Monte Carlo methods. The calculations for the spherical particle where surface magnetic moments are different from bulk ones are performed.

The results reveal throttle structure with increasing surface anisotropy, as well as a significant decrease of the Curie temperature of the NPs as compared to that of the bulk maghemite. This difference can be due to the effects either of the



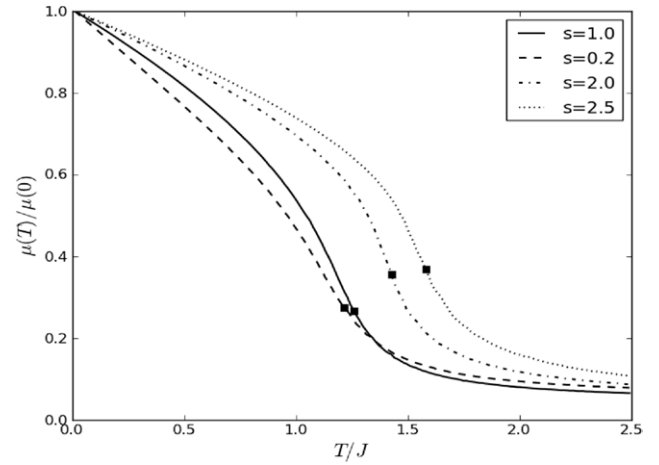
**Figure 8.** Dependence of the full magnetic moment of the NP (normalized to one atom) on  $1/N^{1/3}$  ( $N$  is the number of atoms) for the spherical particle with different surface moments ( $s$  values) and temperature  $T = 0.3 J$ . Dashed lines are linear fits.

coverage of magnetite NPs or of the surface anisotropy (see also the discussion of the microscopic magnetite model with the account of various anisotropic contributions [29]). From the Hamiltonian model (as a part of the classical Heisenberg one) it follows:

$$H = -\frac{J}{2} \sum_{\langle i,j \rangle} \mathbf{S}_i \cdot \mathbf{S}_j \quad (1)$$

where  $\langle i, j \rangle$  denotes nearest-neighbor sites of the spherical particle, and  $\mathbf{S}_i$  is the atomic magnetic moment. Magnetic moments of atoms located in the bulk of the particles are normalized by unity,  $|\mathbf{S}_i| = 1$ , whereas on the surface  $|\mathbf{S}_i| = s$ , where  $s$  is allowed to be different from 1 (the possible difference in exchange parameters for bulk and surface bonds can be taken into account by rescaling  $s$ ). The spherical particle with the radius  $R$  can be defined as a region of simple cubic lattice by inequality:  $|\mathbf{r}_i| < R$ , where  $\mathbf{r}_i$  is lattice sites. Then surface layer is defined by inequality:  $R - a < |\mathbf{r}_i| < R$ , where  $a$  is the lattice constant. However, it was found that these definitions lead to strong ‘geometrical’ oscillations of the number of surface atoms  $N_s$ , which make the subsequent interpretation of the Monte Carlo results difficult. To reduce  $N_s$  fluctuations, the definitions were modified by introducing a weak randomness. Specifically, the substitution  $R \rightarrow R + x$  is made, where  $x$  is a normally distributed variable with zero mean value and with standard deviation of  $\sigma = 0.2$ .

The Monte Carlo simulation was performed by the modified heat bath algorithm [34] using the ALPS library [35]. The  $N$ -dependence of the full magnetic moment at the temperature  $T = 0.3 J$  which is lower than the Curie temperatures for all  $N$  under consideration is shown in figure 8. It is clear from the figure that if  $s = 1$  the finite-size effects alone cannot provide a visible  $N$ -dependence for  $N > 1000$ . With the increase of  $N$  the full magnetic moment decreases for  $s > 1$  and increases for  $s < 1$ . These dependences are in accordance with data presented in figures 1 and 2. Also, a quantitative correlation with the Weizsäcker model [8] is observed.



**Figure 9.** Typical temperature dependences of the magnetic moment of a NP containing  $N = 515$  atoms with different surface moments ( $s$  values).

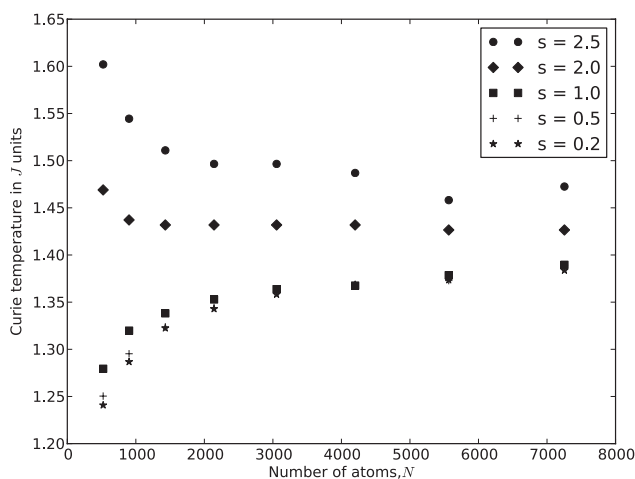
As shown in figure 9, the dependence of magnetic moment at low temperatures is linear as well as in an infinite classical system (in the quantum case this behavior is modified, but not reduced to the usual  $T^{3/2}$  Bloch law [36, 37]). However, the coefficient characterizing this dependence considerably changes with  $s$ .

Note that for the finite systems the temperature dependence of the magnetic moment can be modified in accordance with the discreteness of the magnon spectrum (resulting, in particular, in the energy gap) and the lowering of the mean value of nearest neighbors [36]. As demonstrated by the performed Monte Carlo calculations for both open and periodic boundary conditions, the latter effect predominates. The dependence  $\mu(T)$  is also changed with corresponding changes in the surface anisotropy, as the Monte Carlo results show [38].

It should be stressed that the change in the temperature of the magnetic moment of finite NPs can be substantially different from that in the predictions of the spin wave theory (SWT), so that the real  $T_C$  may be considerably lower than that given by SWT. The finding seems to be similar to that for the infinite layered magnets where the self-consistent spin wave theory (SSWT) yields the decrease of  $T_C$  by about 30–50% [39, 40]. (At the same time, SSWT still overestimates  $T_C$  in comparison with the Monte Carlo calculations, see e.g. figure 5 of [41].) Further decrease of  $T_C$  may be obtained in the field-theoretical approaches, which are especially efficient in the case of low  $T_C$  [40].

The Curie temperature  $T_C$  of the observed finite system (see figure 10) was determined as a temperature where fluctuations of the particle magnetic moment are the strongest. As a measure of these fluctuations, the quantity:  $\langle \mu^2 \rangle - \langle |\mu| \rangle^2$  is used, where  $\mu$  is the full magnetic moment of the particle. The  $N$ -dependence of the Curie temperature can be quite strong, with  $T_C$  decrease for  $s \leq 1$  and increase for  $s > 1$ . The  $N$ -dependence of  $T_C$  is found to be stronger than that of the magnetic moment.

Moreover, it was not expected that the  $N$ -dependence of the Curie temperature would not be monotonous for  $s > 1$ .



**Figure 10.** Dependence of the Curie temperature on the number of atoms in the spherical particle for different  $s$  values.

This non-monotonous behavior can result from the competition of two factors: a reduced coordination number of the surface atoms, which favors disorder and the increase of individual magnetic moments of the surface atoms, which favors ordering. Although the maximal value of  $N$  achieved in the simulations does not cover the whole investigated  $N$ -region, the calculations qualitatively reproduce the experimental behavior of the Curie temperature and a magnetic moment. Moreover, received Monte Carlo results provide some quantitative estimation, unlike those received using the phenomenological Weizsäcker model approach [8].

## 5. Conclusions

The impact of the size of a magnetite cluster on its magnetic properties (magnetic moment, the Curie temperature, blocking temperature, etc) has been studied. The application of the magnetic separation and centrifugation methods for the aqueous biocompatible iron oxide nanoparticles (NPs) allow production of a ‘monodisperse’ fraction of NPs with different diameters (4 – 22 nm), which have been examined by laser correlation spectroscopy, transmission electron microscopy and x-ray diffractometry. For the first time, the method of laser correlation spectroscopy has been applied in real time for the separation and control of NP sizes in aqueous suspensions. Both intact NPs and those covered with a bioresorbable layer have been investigated. The results obtained are interpreted on the basis of Monte Carlo simulations for the microscopic Heisenberg model. All the results obtained are in qualitative correlation.

It has been demonstrated experimentally and by theoretical modeling that the magnetic properties of magnetite NPs were determined not only by their sizes, but also by their surface spin states, while both a growing and falling relationship of the magnetic moment (per  $\text{Fe}_3\text{O}_4$  formula unit) is possible, depending on the number of magnetic atoms in the NP. The combination of the informative methods of magnetic diagnostics with phenomenological and microscopic models for NPs

allows one to obtain the relationship of the specific magnetic moment of NPs with the number of its constituent magnetic formula units, as well as defining the contributions from the bulk and surface states to magnetization. For the first time, both the experimental and theoretical temperature relationship of the magnetic properties of magnetite NPs with different sizes, and of the bulk  $\text{Fe}_3\text{O}_4$  sample, have been obtained and compared.

Both intact NPs and those covered with a bioresorbable layer have been investigated. The type of NP coating affects a number of physical characteristics of the studied NPs, in particular, their magnetic properties. Using the Langevin formula analysis of the magnetization curves  $M(H)$  for the suspension of superparamagnetic NPs, the magnetic moment per one NP could be calculated. The relationship of the magnetic moment per one formula unit for the magnetite NPs with a dextran shell has decaying character with the increase of the number of formula units  $N$ , while the magnetite NPs in the polymer matrix demonstrate the opposite effect.

The change in the NP size controlled by the DLS method causes the change in the Curie temperature and in the magnetic moment of NPs. With the decrease of the nanoparticle diameter, the Curie temperature decreased sharply. The relationship of the size of the magnetic moment with the size of magnetite NPs defines the value of the Curie temperature which is substantially lower than for the bulk samples. Unlike ‘ideal’ NPs with identical bulk and surface individual magnetic moments, the calculated relationship of the magnetic properties in the core-shell model is found to be quite strong. As regards potential applications of these findings, they could be used in medicine, biotechnology, materials science and in forensic applications [42, 43].

## Acknowledgments

This work is, in part, supported by the Program of Fundamental Research of the RAS Physical Division, project no. 15-8-2-9 and by the ‘Dynasty’ foundation. The numerical calculations were performed using the «Uran» supercomputer of the Institute of Mathematics and Mechanics (the Urals Branch of the RAS).

## References

- [1] Li Z M, Shen J, Sun X M and Wang Y J 2013 *Laser Phys. Lett.* **10** 095701
- [2] Tanev S, Tuchin V V and Paddon P 2006 *Laser Phys. Lett.* **3** 594
- [3] Pustovalov V K and Babenko V A 2004 *Laser Phys. Lett.* **1** 516
- [4] 2001 *Nanoscale Materials in Chemistry* ed K J Klabunde (New York: Wiley)
- [5] Schmid E (ed) 2004 *Nanoparticles: from Theory to Application* (Weinheim: Wiley-VCH)
- [6] Battle X and Labarta A 2002 *J. Phys. D: Appl. Phys.* **35** R15
- [7] Nikiforov V N and Filinova E Yu 2009 *Biomedical Application of Magnetic Nanoparticles* (Weinheim: Wiley-VCH) pp 393–455



- [8] Nikiforov V N, Oxengendler B L, Turaeva N N, Nikiforov A V and Sredin V G 2011 *J. Phys.: Conf. Ser.* **291** 012009  
Nikiforov V N et al 2012 arXiv:1206.6985
- [9] Suzdalev P 2006 *Physical Chemistry of Nanoclusters, Nanostructures and Nanomaterials* (Moscow: Com.Kniga) (in Russian)
- [10] Pool Ch and Owens F 2007 *Introduction to Nanotechnology* (New York: Wiley-Interscience)
- [11] Kellermann G and Graievich A 2002 *Phys. Rev. B* **65** 134204
- [12] Kellermann G and Graievich A 2008 *Phys. Rev. B* **78** 054106
- [13] Pakarinen J, Backman M, Djurabekova F and Nordlund K 2009 *Phys. Rev. B* **79** 085426
- [14] Gubin S P, Koksharov J A, Homutov G B and Jurkov G J 2005 *Usp. Khim.* **74** 539 (2005 *Russ. Chem. Rev.* **74** 489)
- [15] Brusentsov N A et al 2004 *J. Mag. Magn. Mater.* **272–276** 2350
- [16] Autenshlyus A I, Brusentsov N A and Lockshin A 1993 *J. Mag. Magn. Mater.* **122** 360
- [17] Brusentsova T N, Brusentsov N A, Kuznetsov V D and Nikiforov V N 2005 *J. Mag. Magn. Mater.* **293** 298
- [18] Khomutov G B 2008 *Nanomaterials for Application in Medicine and Biology* ed M Giersig and G B Khomutov (Dordrecht: Springer) pp 39–58
- [19] Novakova A A, Lanchinskaya V Y, Volkov A V, Gendler T S, Kiseleva T Y, Moskvina M A and Zezin S B 2003 *J. Mag. Magn. Mater.* **258** 354
- [20] Nikiforov V N, Koksharov Yu A, Polyakov S N, Malakho A P, Volkov A V, Moskvina M A, Khomutov G B and Irkhin V Yu 2013 *J. Alloys Compd.* **58** 569
- [21] Nikiforov V N, Kuznetsov V D, Nechipurenko Yu D, Salyanov V I and Evdokimov Yu M 2005 *JETP Lett.* **81** 327  
Nikiforov V N et al 2009 *Nanotechnology International Forum* (Luxembourg: EUR-OP) p 254 (in Russian)
- [22] Brymora K and Calvayrac F 2012 arXiv:cond-mat/1205.1842
- [23] Siegman H C 1992 *J. Phys.: Condens. Matter* **4** 8395
- [24] Dormann J L, Fiorani D and Tronc D 1997 *Adv. Chem. Phys.* **98** 283
- [25] Berkowitz A E, Shuele W J and Flanders P J 1968 *J. Appl. Phys.* **39** 1261
- [26] Coey J M D 1971 *Phys. Rev. Lett.* **27** 1140
- [27] Dimitrov D A and Wysin G M 1994 *Phys. Rev. B* **50** 3077
- [28] Leite V S and Figueiredo W 2006 *Braz. J. Phys.* **36** 652
- [29] Mazo-Zuluaga J, Restrepo J and Mejia-Lopez J 2008 *J. Appl. Phys.* **103** 113906
- [30] Kechrakos D 2010 *Handbook of Nanophysics* vol 3, ed K Sattler (Boca Raton, FL: Taylor and Francis)
- [31] Vedmedenko E Y, Mikuszeit N, Stapelfeldt N, Wieser R, Potthoff M, Lichtenstein A I and Wiesendanger R 2011 *Eur. Phys. J. B* **80** 331
- [32] Labaye Y, Crisan O, Berger L, Greneche J M and Coey J M D 2002 *J. Appl. Phys.* **91** 8715
- [33] Restrepo J, Labaye Y and Greneche J M 2006 *Physica B* **384** 221
- [34] Loison D, Qin C L, Schotte K D and Jin X F 2004 *Eur. Phys. J. B* **41** 395
- [35] Bauer B et al (ALPS collaboration) 2011 *J. Stat. Mech.* **P05001**
- [36] Hendriksen P V, Linderroth S and Lindgard P A 1992 *Phys. Rev. B* **48** 7259
- [37] Kodama R H 1999 *J. Mag. Magn. Mater.* **200** 359
- [38] Trohidou K N 2005 Monte Carlo studies of surface and interface effects in magnetic nanoparticles *Surface Effects in Magnetic Nanoparticles* ed D Fiorani (New York: Springer)
- [39] Irkhin V Yu, Katanin A A and Katsnelson M I 1995 *Fiz. Met. Metalloved.* **79** 65 (*Phys. Met. Metallogr.* **79** 42)
- [40] Katanin A A and Irkhin V Yu 2007 *Phys.-Usp.* **50** 613
- [41] Ignatenko A N, Katanin A A and Irkhin V Yu 2013 *JETP Lett.* **97** 209
- [42] Wiltshcko R and Wiltshcko W 1995 *Magnetic Orientation in Animals* (Berlin: Springer)
- [43] Kirschvink J L 1989 *Bioelectromagnetics* **10** 239